



Preliminary Characterization of a Single Photon Counting System for CT Applications

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- Experimental setup
- Tomographic reconstruction
- Results
- Conclusions and future work



Detection system

Experimental setup

Tomographic reconstruction

Results

Conclusions



Based on the Medipix2 chip Detector 1 mm Si $V_{dep} = 240 V$ Produced by ITC-irst – Trento (Italy) Bump-bonded by VTT (Finland)

- 256 x 256 square pixel matrix (size 55 μm)
- Spatial resolution @ 10% MTF: 17 lp/mm
- Total active area: 14 x 14 mm²
- 13 bit pixel counter
- Max. count rate per pixel 1 MHz
- Electronic noise (sigma) 105 e⁻
- Window threshold discriminator (low and high level)
- Radiation tolerance <200 krad (10 keV X-ray)



The MicroCT prototype



Tomographic acquisition



Experimental setup

Tomographic reconstruction

Results

Conclusions

- Linear scanning is required to enlarge the FoV
- The cone-angle is small (~ 2°), so fan-beam reconstruction is suitable
- Typical acquisition parameters:
 - 30 kVp, 0.5 mAs/view
 - 1 mm Al filtration
 - 480 angles over 360°
 - Magnification factor ranging from 1.2 to 2.9



Phantom for PSF measurement

Experimental setup

Tomographic reconstruction

Results

Conclusions



- A tungsten wire (20 micron)
- Plastic cylinder empty or filled with water
- 3 cm outer diameter, 1 mm wall thickness



Tomographic reconstruction





Spatial resolution: modeling the PSF

• We model the in-plane PSF as a 2D Gaussian function of width σ_{PSF} :

Experimental setup

 $\sigma_{\mathsf{PSF}} = \sqrt{\left(\frac{1}{m}\sigma_{\mathsf{det}}\right)^2 + \left[\left(1 - \frac{1}{m}\right)\sigma_{\mathsf{foc}}\right]^2 + \left(\frac{1}{m}\sigma_{\mathsf{alg}}\right)^2}$

Tomographic reconstruction

 $m = \frac{D_1 + D_2}{D_1}$

where

Results

Conclusions

is the magnification factor.

• The resulting MTF is a Gaussian of width σ_{MTF} :

$$\sigma_{\rm MTF} = \frac{1}{2\pi\sigma_{\rm PSF}} ;$$

$$f_{10\%} = \sigma_{\mathrm{MTF}} \sqrt{2 \mathrm{ln} 10}$$
 .



PSF components

• σ_{det} and σ_{foc} were measured with the slit technique (30 kVp, 0.25 mA): $\sigma_{det} = 22.5 \ \mu m \ (\pm 5\%)$

 $\sigma_{\rm foc} = 9 \pm 2 \ \mu m$

Experimental setup

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• The blurring due to the linear interpolation involved in the reconstruction process can be modeled as follows:

 $MTF_{interp} = |sinc^2(f \cdot \Delta x)|, \quad \Delta x = reconstruction pixel size;$

corresponding to a triangle convolution kernel with FWHM = Δx .

• Approximating the triangle function with a gaussian, we can write:

 $\sigma_{\rm interp} pprox \Delta x$ / 2.35.

• If ramp filter is used, no further blurring is introduced by the reconstruction algorithm:

 $\sigma_{alg} = \sigma_{interp}$ (for FBP reconstruction with ramp filter)

MTF measurement



Reconstruction of W wire (PSF)

Gaussian fit of the profile



Tomographic reconstruction





Results

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Determination of $f_{10\%}$







Spatial resolution of the tomographic system



Tomographic reconstruction

Results

Conclusions





Application: Bone studies on small animals

• We have imaged the finger joint of a chicken

Experimental setup

Tomographic reconstruction

- 60 kVp, 0.3 mAs/view, 1 mm Al filter Energy window: 12-15 keV
- The system is able to resolve the internal structure of bones



Results

Conclusions



Application: Bone studies on small animals

Experimental setup

Tomographic reconstruction

Results

Conclusions





Coronal





Conclusions and future work

Experimental setup

Tomographic reconstruction

Results

Conclusions

 We have characterized a MicroCT scanner prototype based on a Single Photon Counting detection system in terms of spatial resolution.

According to the theory, we obtained resolutions ranging from 11 to 24 lp/mm, for magnification factors ranging from 1.1 to 2.9.

• The system is suitable for high resolution studies on small animals (e.g. bone microstructure).

• We are working on special applications allowed by a Single Photon Counting system (e.g. Dual Energy CT, energy windowing, ecc...).